



University of Verona,  
School of Exercise and Sport Science,  
Laurea magistrale in Scienze motorie preventive ed adattate

Metodologia delle misure delle attività sportive

Wednesday 09/12/2015 h. 8:30÷10

Luca P. Ardigò Ph.D.

# Pedometer

## Final pedometry issues

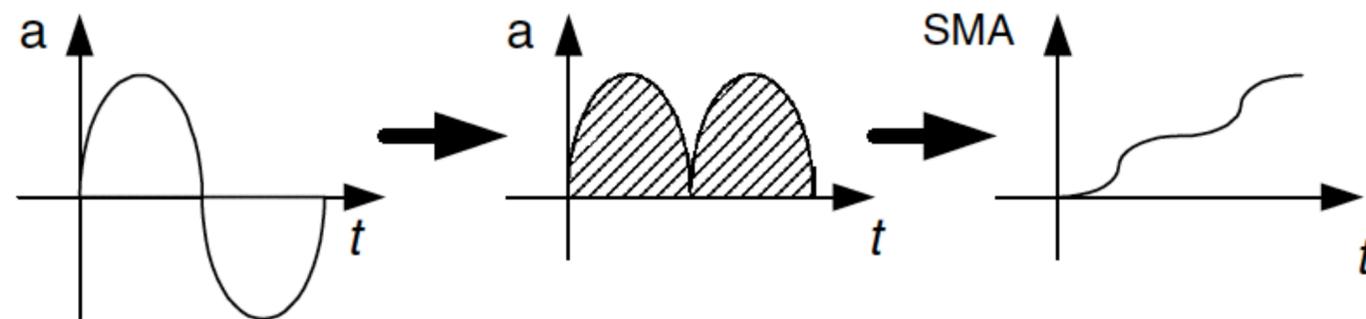
- no discrimination of weight lifting, gradient legged locomotion, cycling, swimming, rowing;
- shoe or ankle accelerometric pedometer -> stride #

# Accelerometer

First generation

Rationale

$a \leftarrow F (= m \times a) \leftarrow$  by paying ME



**Figure 5.** Metabolic energy expenditure (EE) is estimated by computing the signal magnitude area (SMA). The acceleration signal is rectified and then integrated. EE is then estimated by means of a linear regression.

Placement

waist but also chest, back, wrist, ankle

# Accelerometer

- A piezo-electric or -resistive sensor;
- -> "counts" number, intensity;
- no isometric force

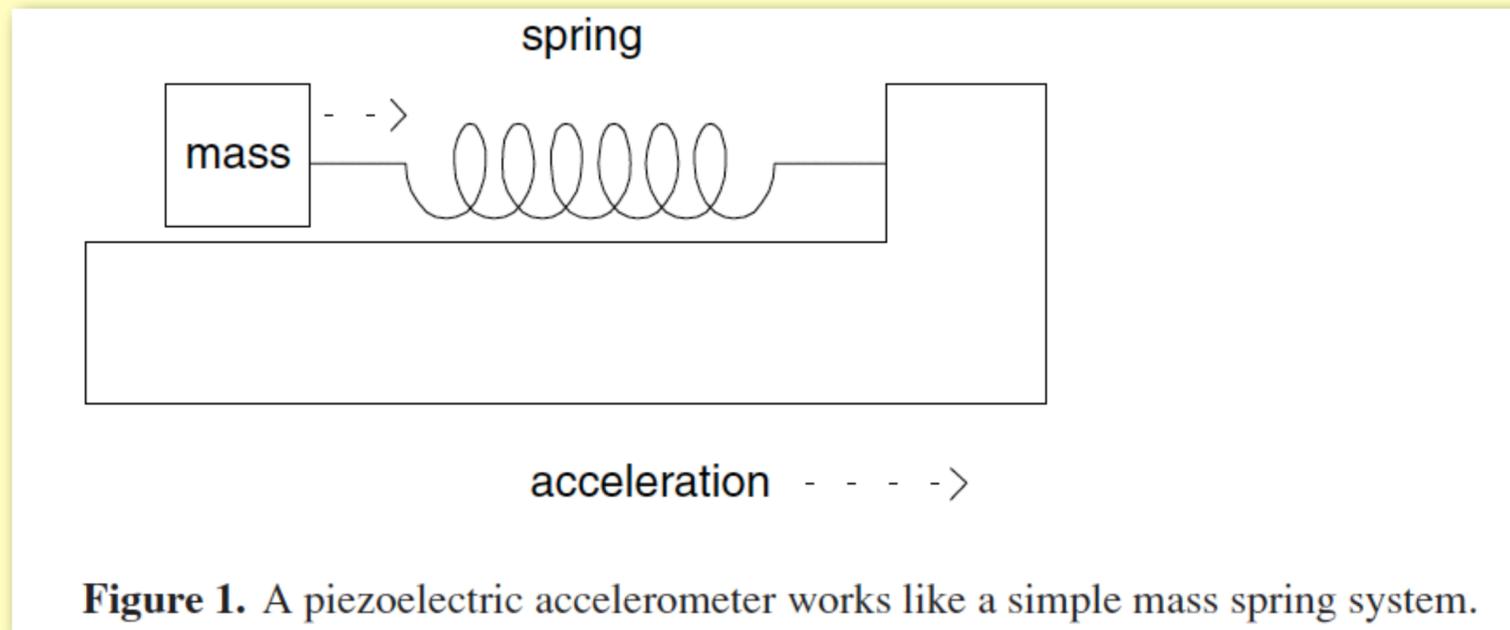
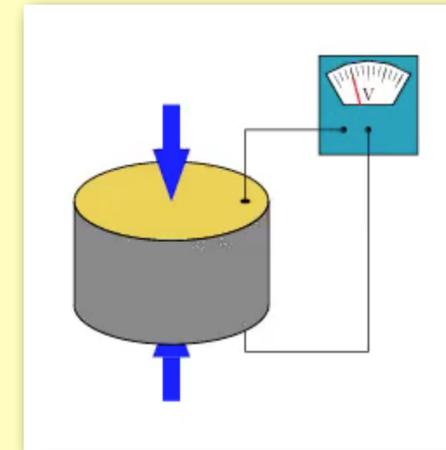
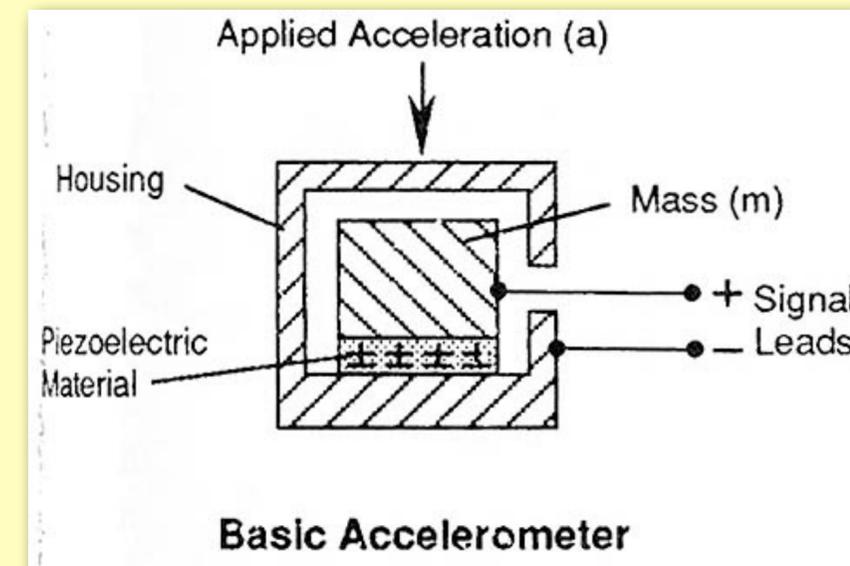
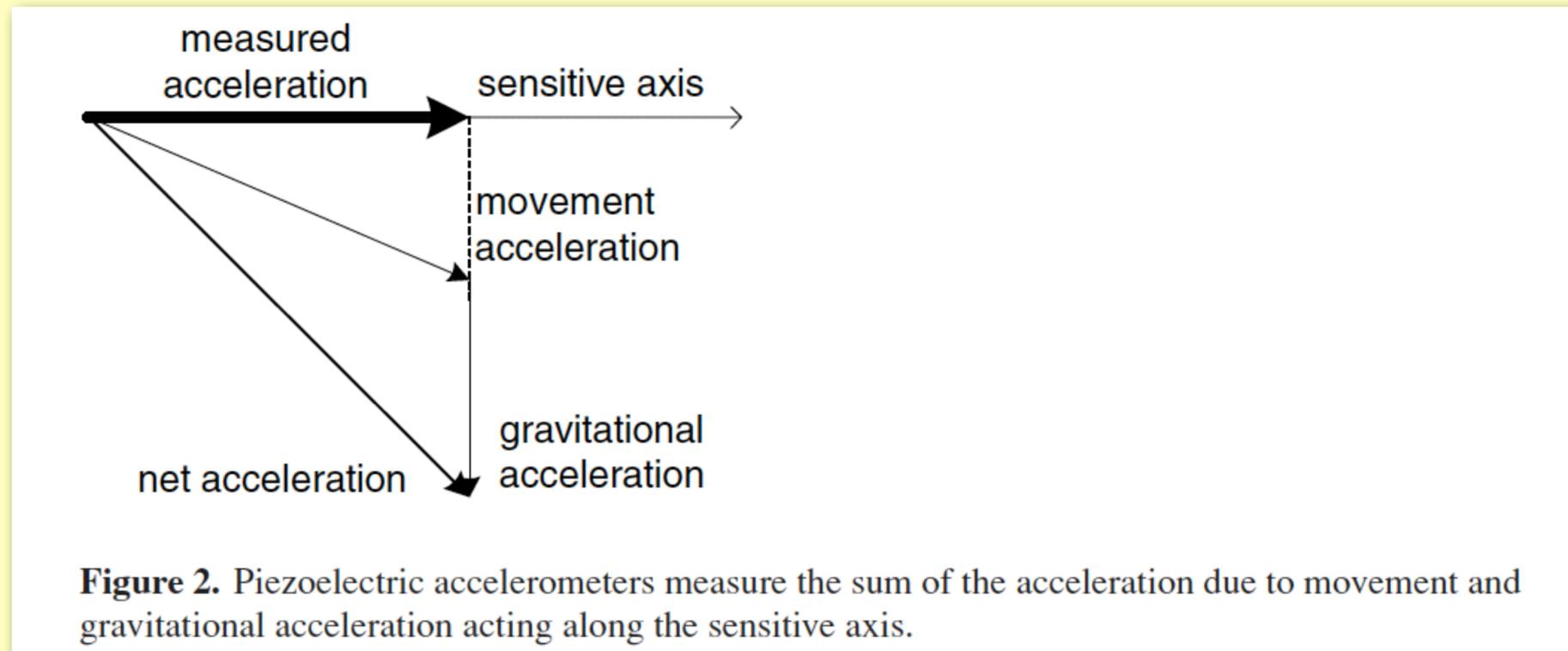


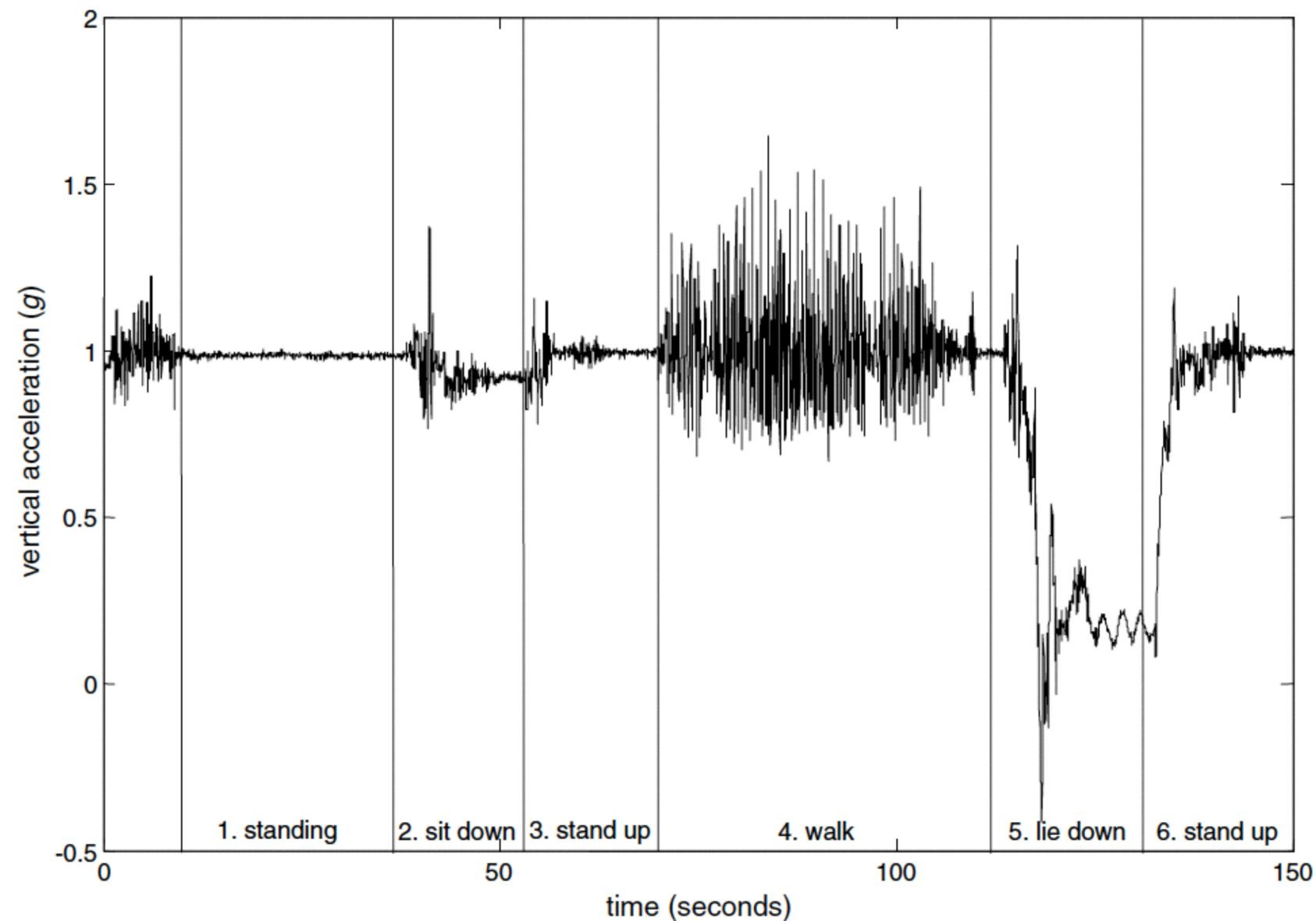
Figure 1. A piezoelectric accelerometer works like a simple mass spring system.



# Accelerometer



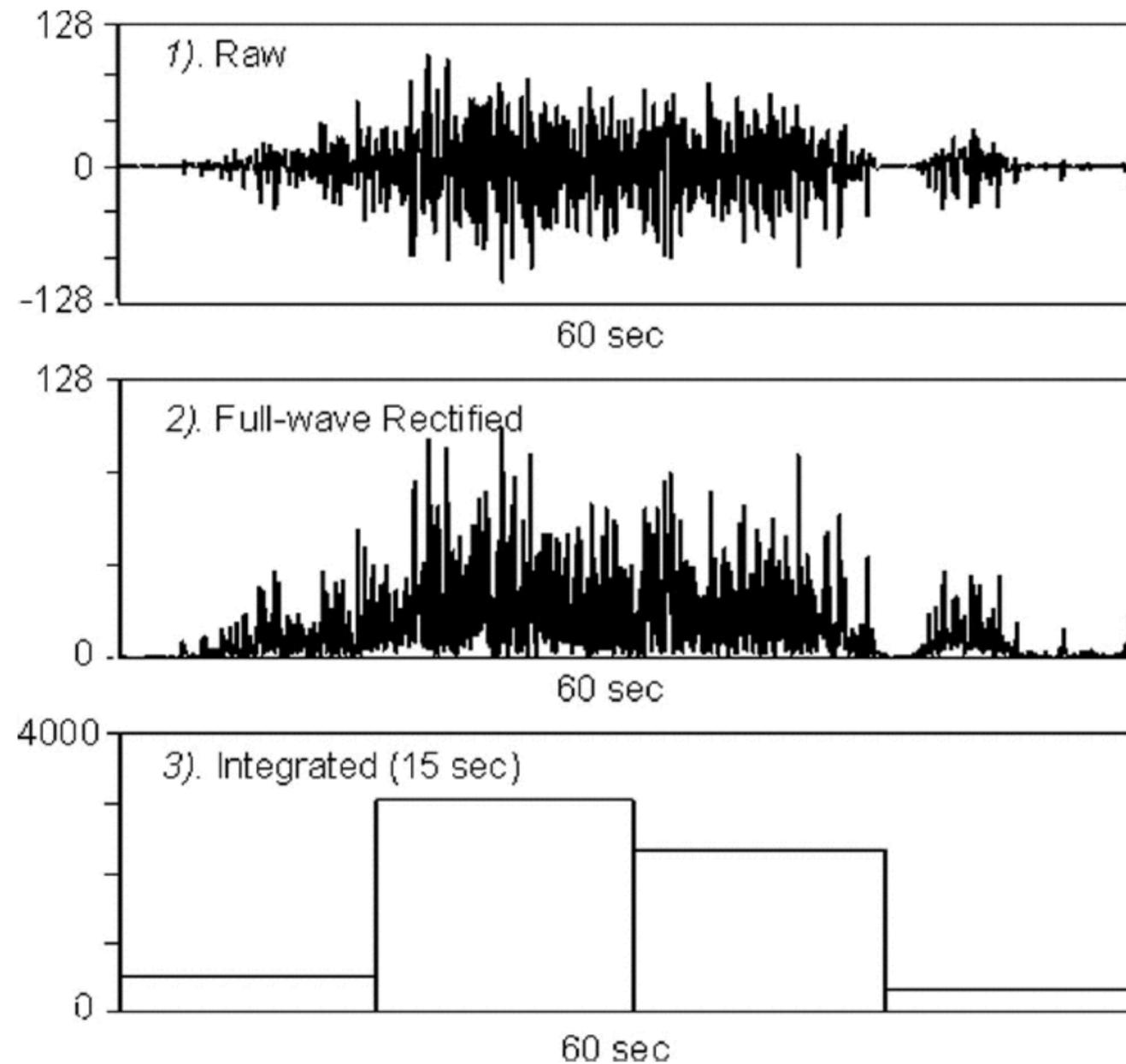
Mathiee et al., 2004



**Figure 4.** Acceleration signal produced by a waist-mounted accelerometer aligned in the vertical (gravitational) direction, during a selection of basic daily movements. The acceleration signal is composed of the gravitational acceleration due to the posture of the subject and the acceleration due to body movement.  $g$  is the acceleration due to gravity, approximately  $9.81 \text{ m s}^{-2}$ . The measured accelerations are dependent on the activity being performed. If the accelerometer was attached at a different point on the body, different acceleration signals would be recorded.

# Accelerometer

measures



**FIGURE 2—Analytical processing of the acceleration data. 1. Raw: a 60-s window of a digitized raw signal collected at 32 Hz and using a 8-bit A/D conversion. 2. Rectification: all negative signal from (1) was turned into positive. 3. Integration: 15-s epochs.**

# Accelerometer

measures

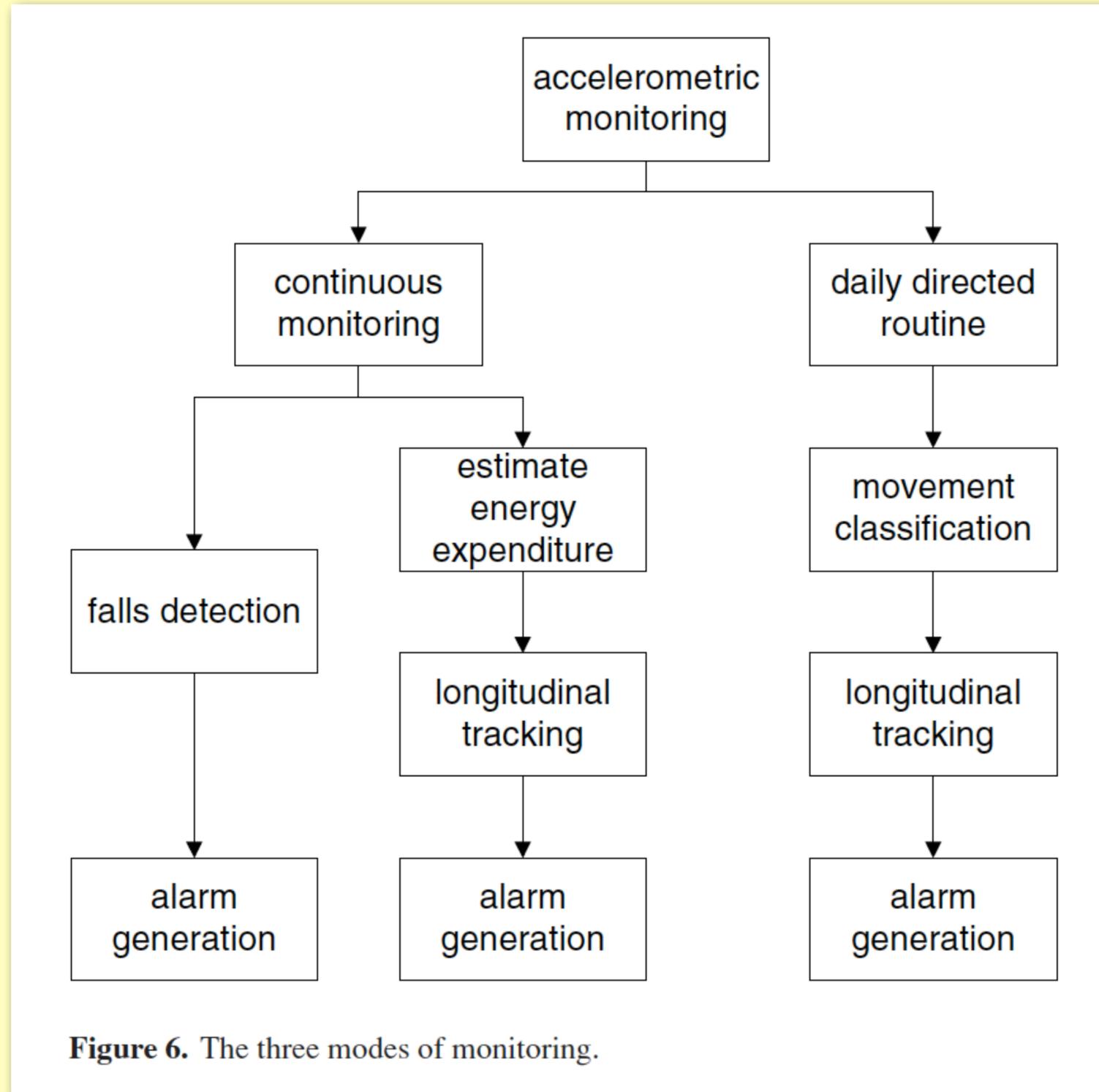


Figure 6. The three modes of monitoring.

# Accelerometer

- Uniaxial accelerometer -> -59% children DLW ME;  
-59÷-50% old men DLW ME;  
+50÷+60% old claudicants DLW ME;  
-59% young women weekly DLW nME;
- Triaxial accelerometer -> +12÷+49%  $\dot{V}O_2$  locomotion ME;  
-21÷-8%  $\dot{V}O_2$  gradient walking ME;  
-68÷-53%  $\dot{V}O_2$  cycling ME;  
-45÷-35%  $\dot{V}O_2$  daily activity ME;  
-35% young women weekly DLW nME

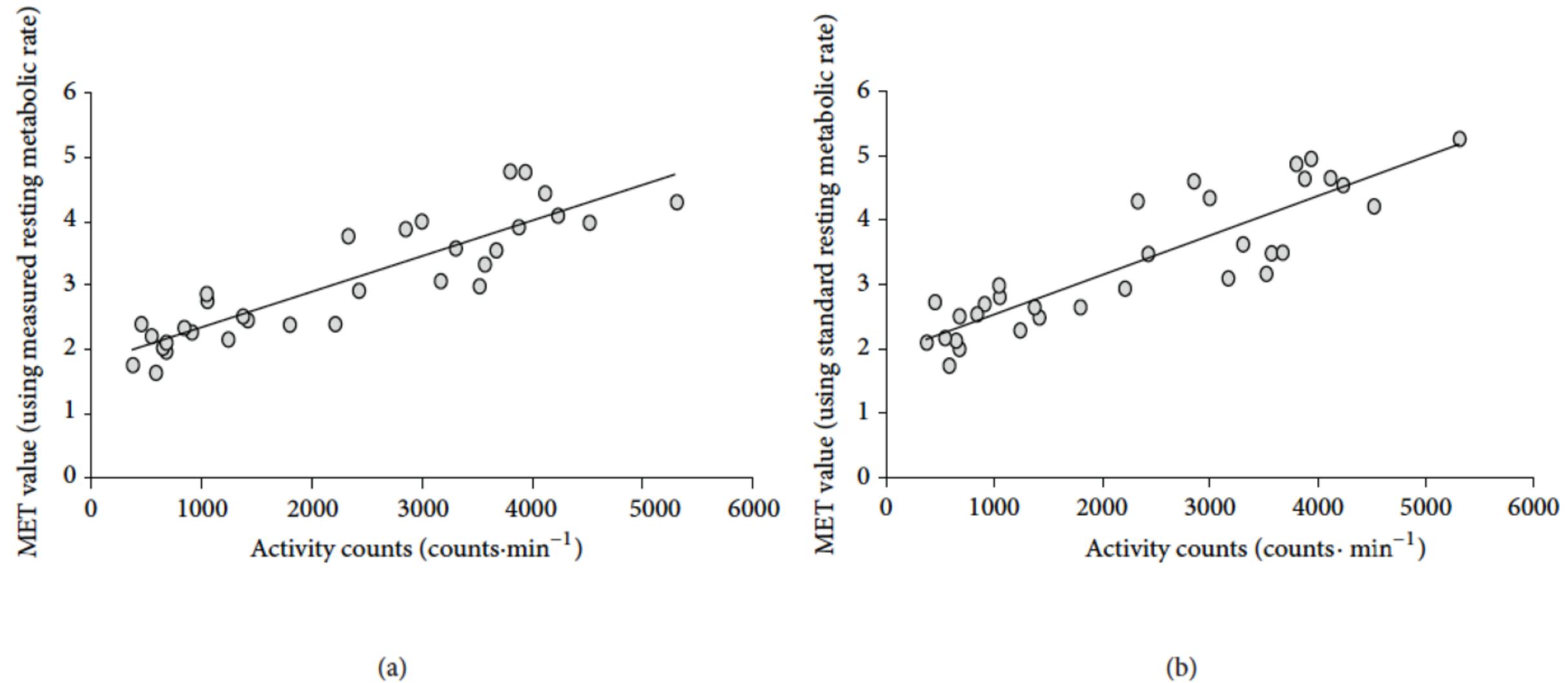


FIGURE 2: (a) Relationship between MET values and activity counts for young group using measured metabolic rate ( $R^2 = 0.80$ , standard error of estimate = 0.40). (b) Relationship between MET values and activity counts for young group using standard (3.5 mL·kg<sup>-1</sup>) metabolic rate ( $R^2 = 0.82$ , standard error of estimate = 0.41).

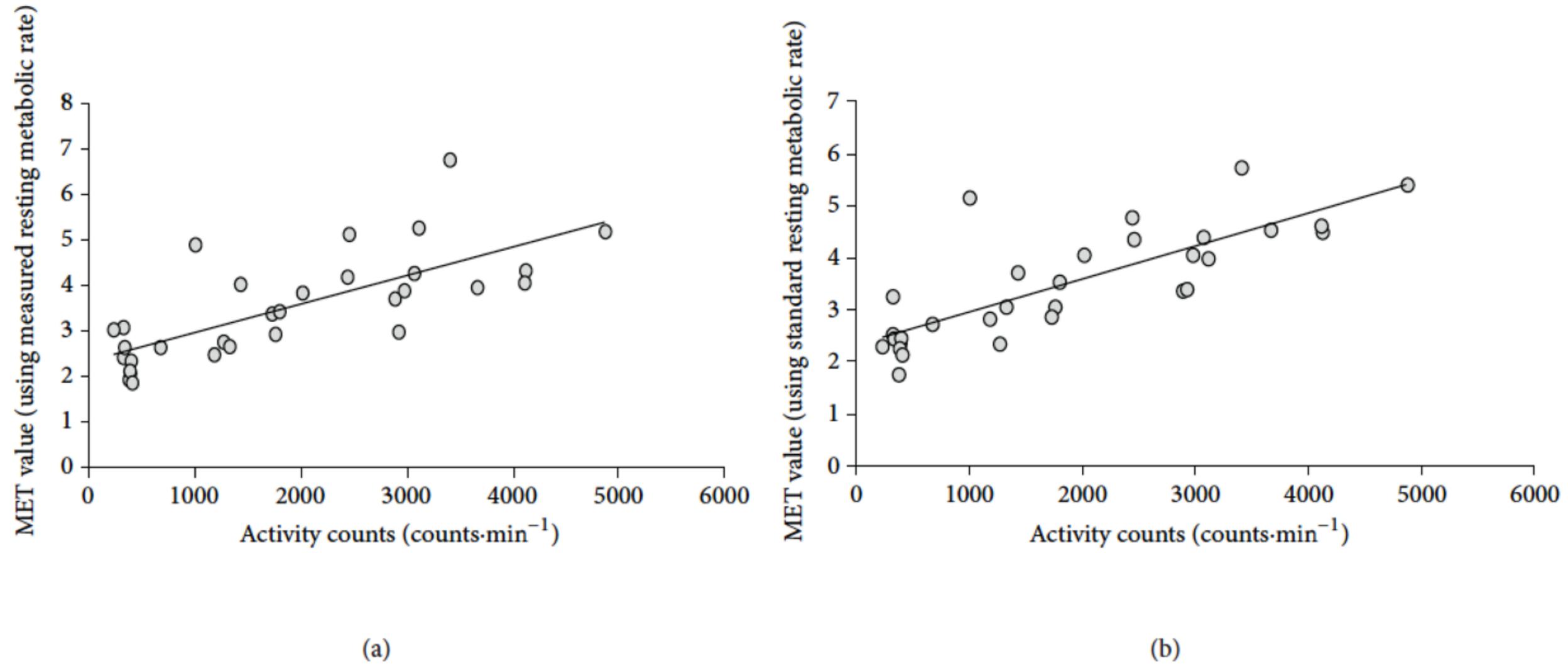


FIGURE 3: (a) Relationship between MET values and activity counts for elderly group using measured metabolic rate ( $R^2 = 0.57$ , standard error of estimate = 0.83). (b) Relationship between MET values and activity counts for elderly group using standard ( $3.5 \text{ mL}\cdot\text{kg}\cdot\text{min}^{-1}$ ) metabolic rate ( $R^2 = 0.52$ , standard error of estimate = 0.85).

# Accelerometer

measures

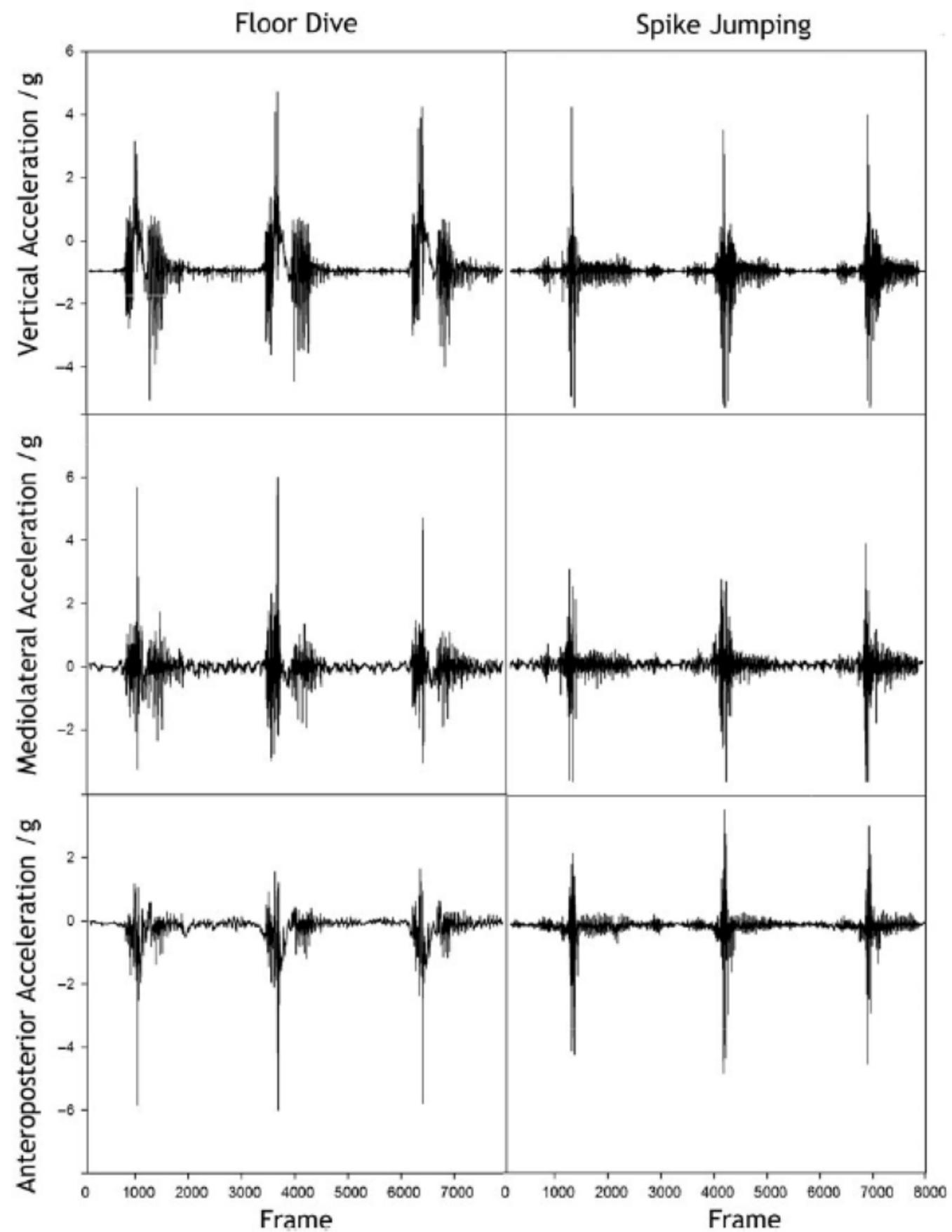


Figure 1. Acceleration in floor dive and spike jump for one randomly selected individual. Acceleration along the vertical, mediolateral and anteroposterior axes are presented in separate boxes.

Janning et al., 2015

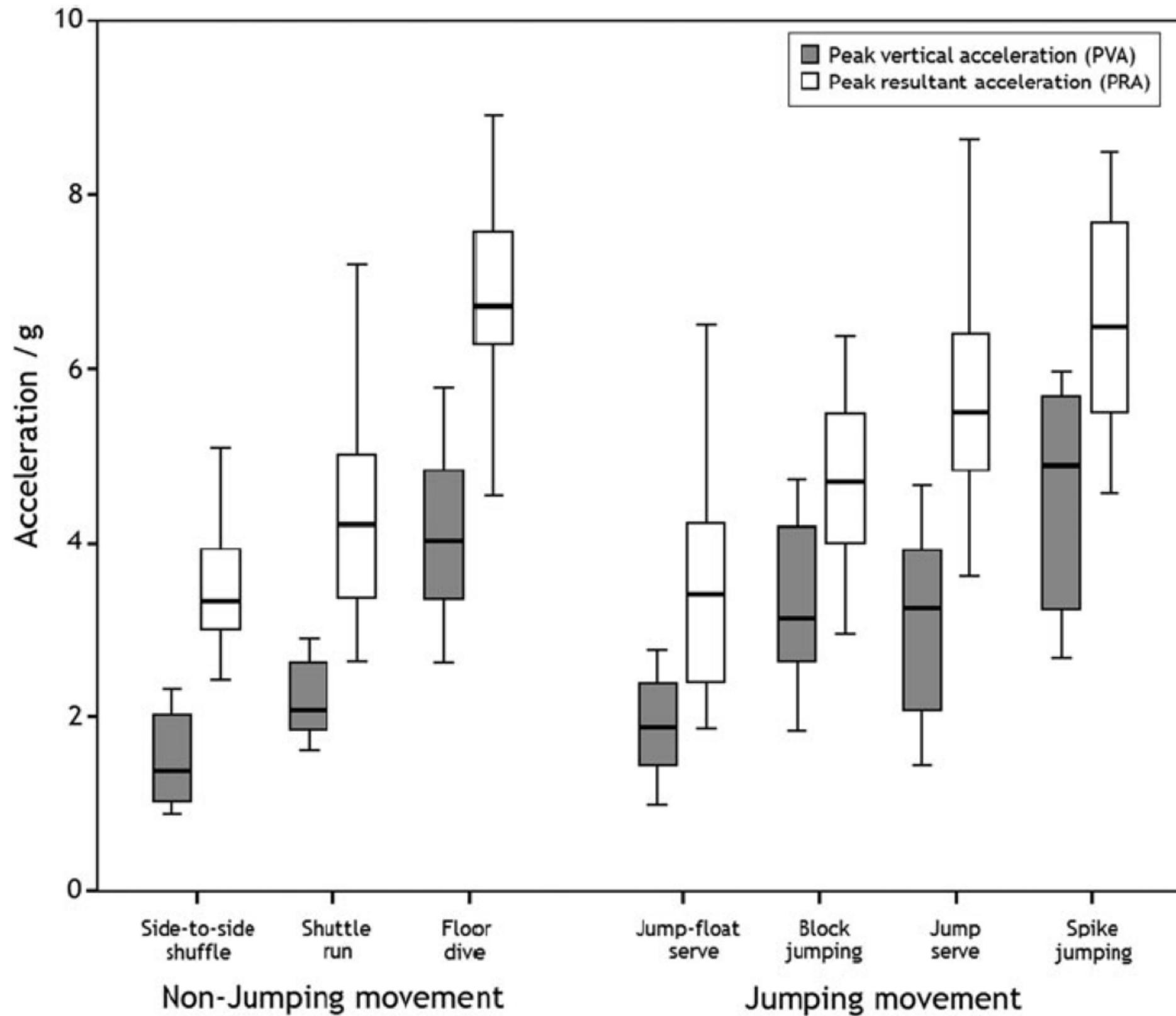


Figure 2. Box-plot showing median (and interquartile range) peak vertical acceleration for non-jumping and jumping volleyball specific movements.

Jarning et al., 2015

measures

# HR wrist monitor

